

Identifying Leukocyte Populations: WOLF Back Scatter Versus Traditional Cytometer Side Scatter

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Introduction

Flow cytometers collect light scatter to measure cellular features, like size and complexity. Traditional cytometers measure small angle scatter, known as forward scatter, to indicate cell size and 90° large angle scatter, known as side scatter, to indicate complexity; this is all measured via a cuvette flow cell. However, the WOLF utilizes a microfluidic flow cell within a disposable cartridge, so it measures some of the light scatter differently.

Forward scatter is collected like a traditional cytometer, but large angle scatter is collected at 180° as back scatter, instead of at 90° as side scatter. Since measuring complexity is critical for flow sorting and analysis, WOLF back scatter was compared to traditional side scatter to confirm equivalent performance.

How Light Scatter Works

Forward scattered light (FSC): Light is scattered by a cell at a very small angle and continues in the same forward direction of its original path (Figure 1). A detector collects this scattered light and translates it into events on a scatter plot. Higher intensity on the plot indicates larger cell size and lower intensity indicates smaller cell size.

Side scattered light (SSC): Light is scattered by a cell at a large angle and travels in a different direction than its original path (Figure 1). A detector measures this at 90° from the original path and represents the difference in cell complexity level (difference in cell membrane, nuclei, secretory granules, etc.) as different event intensities. Higher side scatter indicates greater cell complexity and lower side scatter indicates less cell complexity.

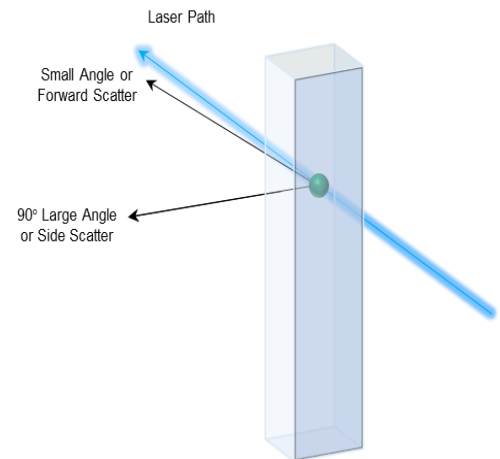


Figure 1. Conventional Optics. A traditional cuvette flow cell measures small-angle forward scatter and 90° large-angle side scatter.

Why the WOLF Uses Back Scatter

Back scattered light (BSC): Light is scattered by a cell at a large angle and collected at 180° from its original path (Figure 2). Like side scatter, back scatter intensity indicates degree of cell complexity.

In a WOLF cartridge, detection at 90° from the laser path is unavailable so side scatter cannot be analyzed. However, detection at 180° is available so back scatter can be measured (Figure 2). This enables cell complexity measurement and may even offer an advantage over SSC for detecting differences in granularity.¹

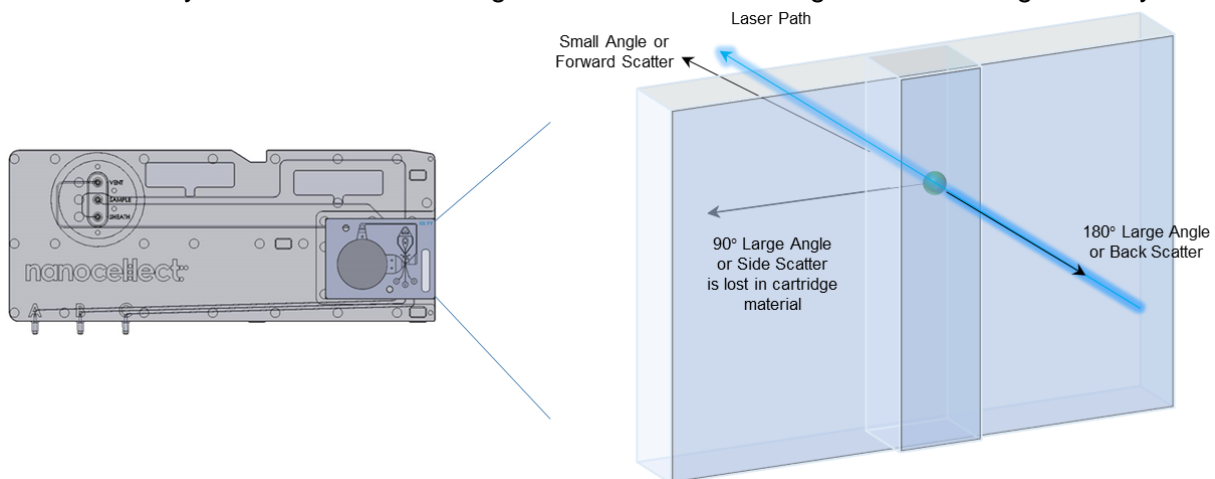


Figure 2. Microfluidic Optics. The WOLF collects small-angle forward scatter like a traditional cuvette flow cell. However, large-angle scatter is collected as BSC at 180° instead of SSC at 90° to accommodate the microfluidic cartridge design.

To confirm that populations appear similarly for back scatter and side scatter, a leukocyte immunophenotyping panel was tested. Leukocyte samples contain three distinct populations differing in size and complexity: lymphocytes, monocytes, and granulocytes. Blood samples from three donors were tested on two WOLF instruments – to eliminate donor, cartridge, and instrument variability – and compared to the ACEA NovoCyte traditional cytometer.

Method

Three whole blood samples were incubated with RBC Lysis Buffer (BioLegend #420301) for 15 min at room temperature (RT) in the dark. They were centrifuged at 350 x g for 5 min and the lysed red cell supernatant was aspirated. Cells were resuspended at 1×10^6 cells/mL in HBSS/2% FBS and incubated for 10 min at RT with True Stain Fc and Monocyte Blockers (BioLegend #422301 and #426101). Antibodies to the following were incubated with cells for 20 min at RT: Monocytes (AF488 Anti-CD14, BioLegend #301817), Granulocytes (PE Anti-CD16, BioLegend #302007), and Lymphocytes (PE-Cy5 Anti-CD3, BioLegend #300410). Cells were washed once and 10,000 events were collected for each sample. Compensation was set with beads (BD #560497) and gates were set with FMOs prior to analysis.

Analysis

Debris and doublets were eliminated with Cells and Singlets gates. For each leukocyte population, negative markers eliminated off-target cells (Figure 4) before the final population-specific marker was gated on and colored to highlight its location on the light scatter plots (Figure 5).

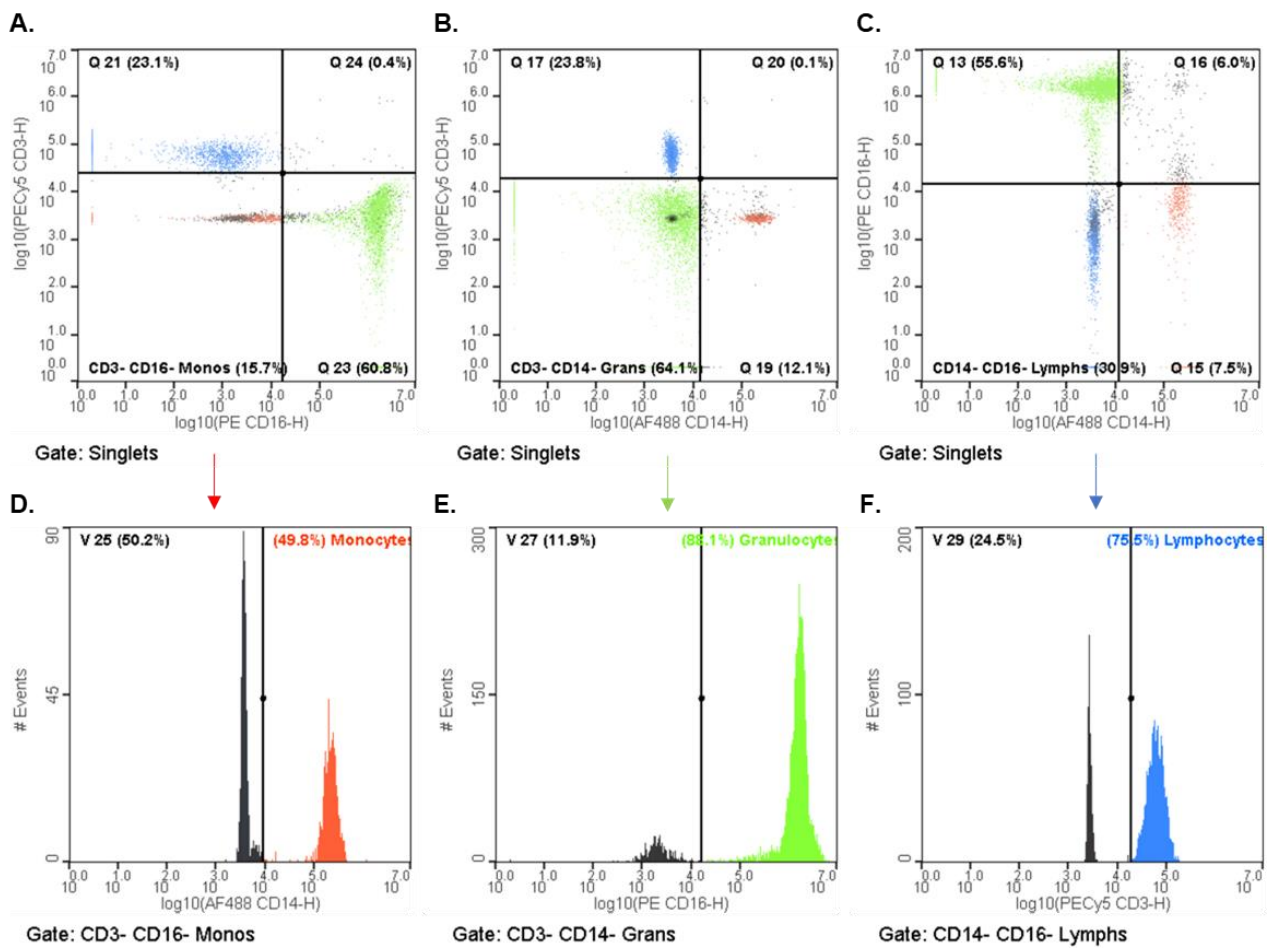


Figure 4. To identify each leukocyte population, negative gates eliminated other cell types before a population-specific gate was applied. (A) To identify monocytes, CD3+ lymphocytes and CD16+ granulocytes were first eliminated. (D) Then, from the CD3-CD16- Monos gate, CD14+ cells were marked as monocytes (red). (B) From the CD3- CD14- Grans gate, CD16+ cells were marked as granulocytes (green) (E). (C) From the CD14- CD16- Lymphs gate, CD3+ cells were marked as lymphocytes (F).

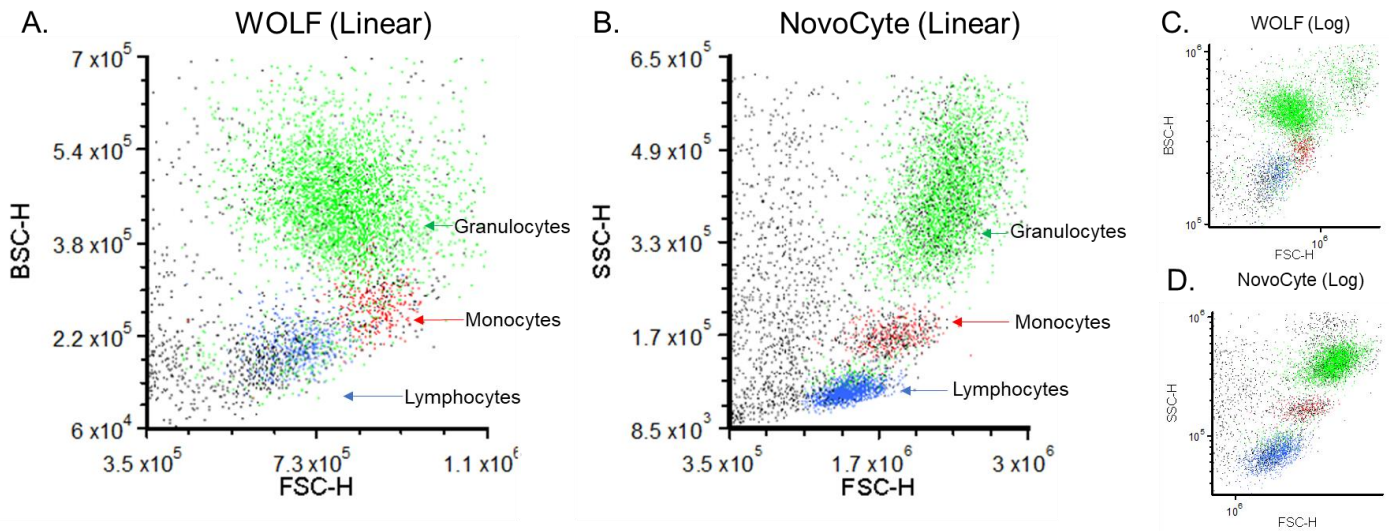


Figure 5. Leukocyte populations on the WOLF are distinct and similarly positioned as on the NovoCyt. The clusters on each plot are colored from the positive populations in Figure 4 (D, E, and F). On both cytometers, lymphocytes present with the lowest granularity, monocytes are in the middle, and granulocytes are most complex with the highest BSC intensity.

Results

The three leukocyte populations appear on the light scatter plots as distinct clusters with similar relative positions on the WOLF and NovoCyt. The WOLF’s back scatter displays the same hierarchy of cell complexity as the NovoCyt’s side scatter: cells increase in granularity from lymphocytes to monocytes to granulocytes. This is true across multiple donors, cartridges, instruments, and for both linear and log plots.

Conclusion

The WOLF’s microfluidic cartridges are disposable to ensure sterile sorting and provide simple fluidic maintenance. Due to this design, the WOLF collects back scatter, which accurately distinguishes cell complexity when compared to a traditional cuvette flow cell. Therefore, users can apply conventional granularity expectations to identify, sort, and analyze cells on the WOLF with the added expectation of superior sterility and ease.

References

1. Kato, H., Nakamura, A., & Kinugasa, S. (2018). Effects of Angular Dependency of Particulate Light Scattering Intensity on Determination of Samples with Bimodal Size Distributions Using Dynamic Light Scattering Methods. *Nanomaterials*, 8(9), 708. doi: 10.3390/nano8090708.